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Diphosphonate Single-Photon Emission Computed Tomography in Cardiac Transthyretin Amyloidosis

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Abstract

**Background:** Planar diphosphonate scintigraphy is an established diagnostic tool for amyloid transthyretin (ATTR) cardiomyopathy. Characterization of the amyloid burden up to the segmental level by single photon emission computed tomography (SPECT) has not been evaluated so far.

**Methods:** Data from consecutive patients undergoing cardiac $^{99m}$Tc-hydroxymethylene diphosphonate ($^{99m}$Tc-HMDP) SPECT and diagnosed with ATTR cardiomyopathy at a tertiary referral center from June 2016 to April 2019 were collected.

**Results:** Thirty-eight patients were included (median age 81 years, 79% men, 92% with wild-type ATTR). In patients with Perugini score 1, the most intense diphosphonate regional uptake was found in septal segments, particularly in infero-septal segments. Among patients scoring 2, the amyloid burden in the septum became more significant, and extended to inferior and apical segments. Finally, patients scoring 3 displayed an intense and widespread tracer uptake. All patients with Perugini score 1 had LGE in at least one antero-septal, one infero-septal, and one infero-lateral segment. All patients with score 2 displayed LGE in infero-septal, inferior, and infero-lateral segments. LGE became extensive in patients scoring 3, with all patients having at least one LGE-positive segment in each region.

**Conclusions:** When assimilating different Perugini grades to evolutive stages of the disease, amyloid deposition seem to progress from the septum to the inferior wall and then to the other regions and from the basis to the apex. The potential of segmental analysis might be particularly relevant in patients with very limited cardiac uptake at planar scintigraphy (Perugini score 1).

Word count: 243 (abstract)
Keywords
Transthyretin amyloidosis, diphosphonate, SPECT, cardiac magnetic resonance

Abbreviation list
ATTR, amyloid transthyretin
CMR, cardiac magnetic resonance
CZT, Cadmium Zinc Telluride
HF, heart failure
LV, left ventricular
SPECT, single photon emission computed tomography
\(^{99m}\text{Tc-HMDP}, \(^{99m}\text{Tc-hydroxymethylene diphosphonate}\)
Introduction

Transthyretin (TTR) is a tetrameric protein synthesized mostly by the liver. As a result of gene mutations or as an ageing-related phenomenon, TTR molecules may misfold and deposit in the heart and in other organs as amyloid fibrils [1]. Cardiac involvement in amyloid TTR (ATTR) amyloidosis typically manifests as left ventricular (LV) pseudohypertrophy and/or heart failure (HF) with preserved ejection fraction. ATTR is increasingly recognized as an underdiagnosed condition [2], as well as a crucial determinant of morbidity and mortality.

Cardiac ATTR can be diagnosed through the demonstration of TTR amyloid deposits on endomyocardial biopsy or following a non-invasive algorithm that includes cardiac magnetic resonance (CMR) and diphosphonate scintigraphy [3]. Planar scintigraphy with the use of $^{99m}$Tc-labelled diphosphonate tracers has proven a valuable tool to detect the presence of myocardial TTR amyloid deposits [4], and to perform a qualitative assessment of the amyloid burden through the Perugini scoring system [5]. Compared to planar imaging, single-photon emission computed tomography (SPECT) examination allows a 3-dimensional assessment of myocardial tracer uptake. Techniques for SPECT imaging are now commonly available, given their role in the diagnostic work-up of coronary artery disease [6], and has been further refined thanks to the introduction of the Cadmium Zinc Telluride (CZT) technique, which allows better spatial resolution and sensitivity [7].

In the present study we evaluated the potential of CZT SPECT imaging for detecting myocardial infiltration in ATTR-related cardiac disease, also in comparison with CMR.

Methods

Patient population

Data from consecutive patients evaluated at a tertiary referral center in Italy from June 2016 to April 2019, undergoing both cardiac diphosphonate scintigraphy with SPECT acquisitions and
CMR as part of their diagnostic workup, and ultimately diagnosed with ATTR cardiomyopathy were retrospectively collected. Cardiac ATTR amyloidosis was diagnosed according to the algorithm by Gillmore et al., whereby histological confirmation and typing of amyloid is not required when patients score 2-3 on the Perugini scale and have no monoclonal protein [3]. Patients provided written informed consent for each examination, as well as data collection and analysis.

**Echocardiographic examination**

Standard, 2-dimensional transthoracic images were obtained using a Philips IE33 Ultrasound machine, with X5-1 transducer (Philips Medical Systems, Palo Alto, California, USA). Standard techniques were used to assess wall thickness, chamber volumes, and indices of systolic and diastolic function, and volumes were measured using the biplane method of disks (modified Simpson's method). The reading protocol was standardized and consistent across years.

**Cardiac magnetic resonance**

All patients without contraindications were examined by a 1.5-T unit (CVi, GE-Healthcare, Milwaukee, USA) using a dedicated cardiac software, 8-channel phased-array surface receiver coil and vectorcardiogram triggering. Ventricular function was assessed by short-axis steady-state free precession cine imaging (field-of-view: 380–400 mm, repetition/echo time: 3.2/1.6 ms, flip angle: 60°, matrix: 224×192, phases: 30, thickness: 8 mm, no gap). LGE imaging was performed 10 to 20 min after gadolinium administration using a segmented T1-weighted gradient-echo inversion-recovery pulse sequence (field-of-view: 380–400 mm, slice thickness: 8 mm, repetition/echo time: 4.6/1.3 ms, flip angle: 208, matrix: 256×192). The inversion time (IT) was individually adapted to suppress the signal of normal remote myocardium (220-300 ms); in all cases, a midventricular short-axis TI-scout sequence was used to choose the appropriate inversion time and to check the presence of paradoxical blood/myocardium inversion times. When no normal myocardium was found, the IT was chosen using conventional values to suppress normal myocardium and make
enhanced myocardium look bright; in such cases, the whole myocardium was nulled before the blood pool in the IT scout sequence.

LV and RV volumes, wall thickness, mass and global function were determined from the stack of short-axis cine by 2 experienced CMR readers (C.G., A.B.), blinded to SPECT results. The presence and pattern of LGE were visually determined on post-contrast short-axis and long-axis images by the same 2 operators; in cases of disagreement, a third operator (G.D.A.) was consulted.

**Scintigraphy examination**

$^{99m}$Tc-hydroxymethylene diposphonate ($^{99m}$Tc-HMDP) was prepared from a commercial kit (OSTEOCIS). Each patient received intravenous 700-740 MBq of $^{99m}$Tc-HMDP, and a whole-body scan (anterior and posterior projections) was performed 150 min later, in a 256*1024 matrix (E.Cam; Siemens Medical Solution; Hoffman Estates, IL, USA). All patients then underwent a CZT tomographic acquisition using a dedicated cardiac camera (Discovery NM 530c; GE Healthcare; Haifa, Israel).

Planar images were acquired with a standard SPECT camera using low-energy, high-resolution collimators and an appropriate scan speed to reach over $2\times10^6$ counts. Cardiac uptake was graded according to the Perugini system as: grade 0, no cardiac uptake; grade 1, cardiac uptake present but less intense than the bone signal; grade 2, cardiac uptake with intensity similar or greater than bone signal; grade 3, cardiac uptake with much attenuated or absent bone signal [8]. All patients then underwent a CZT acquisition, lasting about 6 minutes. The system design enabled a high-quality imaging of a 3-dimensional volume where the patient’s heart was positioned. CZT images were reconstructed on a standard workstation (Xeleris II; GE Healthcare) using a previously validated dedicated iterative algorithm with 50 iterations. A Butterworth post-processing filter (frequency 0.37, order 7) was applied to the reconstructed slices. Images were reconstructed without correction for scatter or attenuation.
Quantitative analysis of tracer uptake was performed using normalized polar maps and a 17-segment LV model. Segmental $^{99m}$Tc-HMDP tracer uptake was calculated as percentage of the peak tracer uptake, and classified using the following scale: 0=normal (<10% uptake), 1=mild increase of tracer uptake (10-29%), 2=moderate increase (30-49%), 3=severe increase (50-69%), 4=very severe increase (70-100%). The following LV regions were also considered: anterior (segments 1, 7), antero-septal (2, 8), infero-septal (3, 9), inferior (4, 10), infero-lateral (5, 11), antero-lateral (6, 12), apical (13-17). For each patient, the average tracer uptake in segments composing each region was calculated.

**Statistical analysis**

Statistical analysis was performed using IBM SPSS Statistics (version 22, 2013). Normal distribution was assessed through the Kolmogorov-Smirnov test; as all variables had non-normal distribution, they were expressed as median and interquartile interval. Differences between groups were tested through the Mann-Whitney U test. Categorical variables were compared by the Chi-square test with Yates correction. p values <0.05 were considered statistically significant.

**Results**

**Study population, echocardiographic and cardiac magnetic resonance findings**

The main characteristics of study population (n=38) are reported in Table 1. Mean age was 81 years, and 30 patients (79%) were men. The vast majority (n=35, 92%) was diagnosed with wild-type ATTR, and 3 (8%) with variant ATTR. Interventricular septum and posterior wall thickness, relative wall thickness (RWT), and E/e’ ratio values were all increased. Among patients undergoing CMR scan (n=35, 92%), median LV ejection fraction was 55% (47-65), and LV mass index was increased (125 g/m$^2$ [99-151]). Three patients (8%) scored 1 on the Perugini scale; the diagnosis was made following demonstration of ATTR amyloid on endomyocardial biopsy (2 patients), or periumbilical fat biopsy (1 patient). Twenty patients (53%) scored 2, and 15 (40%) scored 3. In
parallel with increasing Perugini score values, a progressive increase in wall thickness and RWT, and a trend towards increased LV mass index were noted (Table 1).

Perugini grades vs. SPECT: percent diphosphonate uptake

SPECT imaging was deemed of high quality in all cases. In patients scoring 1 on the Perugini scale (n=3), the most intense diphosphonate uptake was found in septal segments, particularly in infero-septal segments (3 and 9). Antero-septal segments (2 and 8) and the apical septal segment (14) followed, while the lowest uptake was observed in some apical segments, namely apical inferior (15), lateral (16), and apex (17).

Among patients scoring 2 (n=20), the amyloid burden in the septal region became more significant, and extended to the inferior region (segments 4 and 10), and some apical segments (14 and 15). Finally, a diffuse and intense uptake was found in patients scoring 3 (n=15), involving also the anterior, lateral, and apical regions (Figures 1 and 2, Supplemental Figure 1). The basal-to-apical ratio of diphosphonate uptake was lower than in patients scoring 1 or 2, reflecting greater amyloid accumulation in the apical region (Figure 3).

Perugini grades and SPECT vs. LGE analysis

All patients scoring 1 on the Perugini scale had LGE in at least one antero-septal segment (2, 8), one infero-septal segment (3, 9), and one infero-lateral segment (5,11). Conversely, LGE was found in at least 1 apical segment (13-17) in a single patient. Among patients scoring 2, all displayed LGE in the infero-septal, inferior, and infero-lateral regions; among apical segments, the apical septal (14) and apical inferior (15) were those most often showing LGE. When progressing to Perugini grade 3, LGE became extensive, with all patients displaying at least one LGE-positive segment in each region (Supplemental Figure 2). In the whole population, patients with LGE in a segment or region consistently displayed a more intense $^{99mTc}$HMDP uptake than those with no LGE (Supplemental Figure 3). Finally, a good agreement was found between severe or very severe
Discussion

The present study represents the first dedicated assessment of diphosphonate SPECT as a tool for characterizing the segmental amyloid burden in ATTR cardiomyopathy. $^{99m}$Tc-HMDP SPECT allows to estimate the regional amyloid burden and make some assumptions about disease evolution across Perugini stages.

Myocardial scintigraphy with diphosphonate tracers is a pillar of non-invasive diagnosis of ATTR cardiomyopathy [7], given the high specificity of myocardial diphosphonate uptake [10]. This technique is commonly available (as bone scintigraphy), and its contraindications are basically limited to pregnancy or breastfeeding [11], which are extremely rare among patients undergoing diagnostic workup for cardiac ATTR.

Increasing diphosphonate uptake in the heart is associated with an apparent parallel reduction in bone uptake on planar imaging, which forms the basis of the Perugini score [5]. It has hitherto been assumed that the tracer is avidly and competitively taken up by the heart with reciprocal reduction in bone uptake [12]. In other words, patients scoring 1 on the Perugini scale would have a lower amyloid burden than those scoring 2, who in turn would have less cardiac amyloid than those scoring 3. Interestingly, this hypothesis has never been verified through histopathological studies, and tracer kinetics across Perugini scores has never been specifically investigated. When Perugini grades are assimilated to evolutive disease stages, the results of diphosphonate SPECT allow to make some assumptions about the natural history of ATTR cardiomyopathy, by suggesting that amyloid accumulation progresses from the septum to the inferior region, then involves the lateral, anterior, and apical regions. The late involvement of the apex might account for the relative preservation of contractility of the apex (“apical sparing”), which is highly sensitive and specific for cardiac amyloidosis [13].

$^{99m}$Tc-HMDP tracer uptake (>50%) and LGE presence at both segmental and regional level (Supplemental Table 1).
Amyloid deposition leads to an expansion of extracellular spaces, manifesting as LGE at CMR [14]. When assimilating again different Perugini score values to evolutive stages of the disease, we noticed that LGE positivity extended from the septal and inferior regions to the other regions, ultimately involving apical segments, with a similar progression than amyloid accumulation on SPECT imaging. Although segmental LGE patterns were not specifically analyzed, LGE was usually subendocardial or transmural, in agreement with the hypothesis of amyloid deposition starting in subendocardial layers (possibly causing the typical global subendocardial LGE), then expanding towards the subepicardial layers.

Very limited evidence exists about diphosphonate SPECT as an imaging tool for ATTR cardiomyopathy. Following 2 small studies that did not perform a quantification of regional tracer uptake [15,16], 2 studies compared SPECT with another imaging modality, while not performing a quantification of segmental tracer uptake. Sperry et al. evaluated $^{99m}$Tc-pyrophosphate SPECT versus strain echocardiography in a cohort of 54 patients with ATTR (2 with Perugini score 1) [17]. Contrary to that study, we performed an analysis on 17 segments instead of basal, mid-cavity and apical regions, and we compared amyloid burden by SPECT with another 3-dimensional technique, namely CMR. In a similar study by Pradel et al., findings from $^{99m}$Tc-HMDP SPECT and strain echocardiography were compared. No comparison between the different Perugini scores was performed, and no Perugini 1 patients were included [18].

The studies above did not address the added diagnostic value of SPECT to planar scintigraphy. At present, ATTR cardiomyopathy can be diagnosed with no need for endomyocardial biopsy when clinical and imaging findings are compatible with cardiac amyloidosis, no monoclonal protein is found, and planar scintigraphy shows a Perugini grade 2 or 3 uptake [3]. Our data show that an intense myocardial uptake localized to the septum (particularly in the infero-septal segment) can manifest as grade 1 uptake. Therefore, tomographic imaging showing a prominent diphosphonate uptake within the septum or in the infero-septal segment, together with no evidence of monoclonal component, might strengthen the suspicion of ATTR cardiomyopathy. Dedicated studies examining
the diagnostic yield of this approach, and the possibility to avoid the need for histological examination in patients with Perugini score 1 are warranted.

Some limitations of this hypothesis-generating study must be acknowledged. First, 92% of patients scored 2 or 3 on the Perugini scale, reflecting the fact that ATTR cardiomyopathy is usually diagnosed in a relatively advanced stage. Only 8% of patients (n=3) scored 1 on the Perugini scale, although this is the patient subset where SPECT imaging is more likely to show an additive value over planar scintigraphy. Additionally, patients with amyloid light-chain amyloidosis were not evaluated, although they may score 1 on the Perugini scale. Second, segmental and regional $^{99m}$Tc-HMDP uptake is likely influenced by wall thickness, which decreases from the basis to the apex. A normalization of tracer uptake by wall thickness was not performed because CZT SPECT did not allow to measure wall thickness, and we preferred not to use values from CMR examinations. Third, the study had a retrospective, cross-sectional design, and relied on the assumption that Perugini score values could be assimilated to different disease stages. Longitudinal studies with serial SPECT examinations would be needed to track disease progression, possibly also in the perspective of stratifying patient risk and assessing the response to therapy. Fourth, the role of SPECT imaging for diagnostic purposes, and possibly for other applications (such as assessment of the response to treatment), remains to be specifically examined. Fifth, this study focused primarily on SPECT imaging, and tissue characterization by CMR was limited to LGE presence or absence in the 17 LV segments. Nonetheless, amyloidosis is a diffuse disease, and T1 mapping techniques such as native T1 and extracellular volume fraction might have been more informative than LGE.

In conclusion, the intensity of segmental uptake of $^{99m}$Tc-HMDP SPECT varies across Perugini grades. This allows to hypothesize that amyloid deposition progresses from the septum to the inferior wall and then to the other regions and from the basis to the apex, and also that SPECT imaging might have an additive diagnostic value in patients with very limited uptake in the cardiac region at planar scintigraphy (Perugini score 1).
Figure legends

Figure 1. $^{99m}$Tc-hydroxymethylene diphosphonate (HMDP) uptake across Perugini grades: regional analysis.
Colors reflect the intensity of tracer uptake, according to the semiquantitative scale reported in the Methods section.

Figure 2. Regional uptake across Perugini scores.
Single photon emission computed tomography (SPECT) results from 3 patients scoring 1, 2, and 3 on the Perugini scale. Amyloid accumulation, manifesting as $^{99m}$Tc-hydroxymethylene diphosphonate (HMDP) uptake, starts from the infero-septal region and progressively extends to the whole left ventricle, partially sparing the true apex.

Figure 3. Basal-to-apical $^{99m}$Tc-hydroxymethylene diphosphonate (HMDP) uptake across Perugini grades.
Ratios of the average value of $^{99m}$Tc-HMDP uptake in basal segments to average value in apical segments were calculated and plotted as a function of Perugini grades.
References


15. Minutoli F, Di Bella G, Mazzeo A, Donato R, Russo M, Scribano E, Baldari S. Comparison between (99m)Tc-diphosphonate imaging and MRI with late gadolinium enhancement in


Author statement

Chrysanthos Grigoratos: Data curation, Writing- Original draft preparation
Alerto Aimo: Data curation, Writing- Original draft preparation
Claudio Rapezzi: Supervision and Reviewing
Dario Genovesi: Visualization, Investigation, Writing- Reviewing and Editing
Andrea Barison: Visualization, Investigation, Writing- Reviewing and Editing
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Paolo Marzullo: Visualization, Investigation, Writing- Reviewing and Editing
Alessia Gimelli: Visualization, Investigation, Writing- Reviewing and Editing
Michele Emdin: Writing- Reviewing and Editing
### Table 1. Population characteristics.

<table>
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<tr>
<th></th>
<th>Patients n=38</th>
<th>Perugini 1 n=3 (8%)</th>
<th>Perugini 2 n=20 (53%)</th>
<th>Perugini 3 n=15 (40%)</th>
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<tr>
<td><strong>Age (years)</strong></td>
<td>81 (76-83)</td>
<td>76 (76-79)</td>
<td>82 (79-83)</td>
<td>81 (80-84)</td>
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<td><strong>Male sex (n, %)</strong></td>
<td>30 (79)</td>
<td>3 (100)</td>
<td>16 (80)</td>
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<td><strong>BMI (kg/m²)</strong></td>
<td>27.5 (24.3-30.0)</td>
<td>27.9 (26.2-28.7)</td>
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<td><strong>AF (n, %)</strong></td>
<td>13 (43)</td>
<td>1 (33)</td>
<td>7 (35)</td>
<td>6 (40)</td>
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<td><strong>LBBB (n, %)</strong></td>
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<td>0 (0)</td>
<td>2 (13)</td>
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<td><strong>Hemoglobin (g/dL)</strong></td>
<td>12.4 (11.6-13.6)</td>
<td>13.0 (12.7-13.6)</td>
<td>13.1 (11.3-12.9)</td>
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<td><strong>eGFR (mL/min)</strong></td>
<td>52 (44-81)</td>
<td>62 (50-73)</td>
<td>48 (34-62)</td>
<td>56 (49-81)</td>
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<td><strong>NT-proBNP (ng/L)</strong></td>
<td>3690 (1493-7420)</td>
<td>2515 (1677-4870)</td>
<td>5491 (3800-8134)</td>
<td>3652 (1827-9426)</td>
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<td><strong>NYHA I/II/III (n, %)</strong></td>
<td>8/14/16 (21/37/42)</td>
<td>1/1/1 (33/33/33)</td>
<td>4/7/9 (20/35/45)</td>
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<td><strong>ATTRwt/ATTRv (n, %)</strong></td>
<td>35/3 (92/8)</td>
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<td>18/2 (90/10)</td>
<td>14/1 (93/7)</td>
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**Echocardiogram**

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<th>Patients n=38</th>
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<th>Perugini 2 n=20 (53%)</th>
<th>Perugini 3 n=15 (40%)</th>
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<td><strong>IV septal thickness (mm)</strong></td>
<td>19 (16-21)</td>
<td>14 (13-16)</td>
<td>18 (15-20)</td>
<td>21 (19-23)</td>
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<td><strong>PW thickness (mm)</strong></td>
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<td>12 (12-13)</td>
<td>15 (14-18)</td>
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<td><strong>RWT</strong></td>
<td>0.76 (0.62-0.91)</td>
<td>0.45 (0.44-0.51)</td>
<td>0.71 (0.62-0.92)</td>
<td>0.83 (0.75-0.91)</td>
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<td>CMR</td>
<td>LVEDVi (mL/m²)</td>
<td>LVESVi (mL/m²)</td>
<td>LVMI (g/m²)</td>
<td>LVEF (%)</td>
<td>LGE presence (n, %)</td>
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<td></td>
<td>81 (64-96)</td>
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<td>26 (23-36)</td>
<td>109 (94-129)</td>
<td>138 (119-153)</td>
<td>0.054</td>
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</table>

Estimated glomerular filtration rate (eGFR) is calculated through the Chronic Kidney Disease Epidemiology Collaboration (CKD-EPI) equation. AF, atrial fibrillation; ATTRm, mutated transthyretin amyloidosis; ATTRwt, wild-type transthyretin amyloidosis; BMI, body mass index; CMR, cardiac magnetic resonance; ECV, extracellular volume; IV, interventricular; LA, left atrium; LBBB, left bundle branch block; LGE, late gadolinium enhancement; LVEDVi, left ventricular end-diastolic volume index; LVESVi, left ventricular end-systolic volume index; LVEF, left ventricular ejection fraction; LVMI, left ventricular mass index; MI, myocardial infarction; NT-proBNP, N-terminal fraction of pro-brain natriuretic peptide; PW, posterior wall; RA, right atrium; RVEDVi, right ventricular end-diastolic volume; RVEF, right ventricular ejection fraction; RVEDVi, right ventricular end-systolic volume index; RWT, relative wall thickness.
Highlights

- In ATTR cardiomyopathy, SPECT allows to characterize regional amyloid burden.
- SPECT also allows to quantify the intensity of amyloid burden.
- Amyloid deposition begins in the septal and inferior walls and the basal region.